

# Proton MR spectroscopy to assess axonal damage in multiple sclerosis and other white matter disorders

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**Proton MR spectroscopy allows *in vivo* measurement of N-acetylaspartate in white matter, providing a biochemical index of axonal integrity. Several recent studies of patients with multiple sclerosis and other white matter disorders have shown both transient and sustained decreases in N-acetylaspartate in white matter lesions and in brain regions appearing normal on conventional MRI. These data have emphasised that a substantial amount of axonal damage or loss (presumably secondary to myelin pathology) is consistently present in most of these disorders. Recent post-mortem studies support these results. In contrast to changes seen with conventional MR imaging, decreases in N-acetylaspartate have shown a close correlation with changes in neurological status. This suggests that axonal damage may be more relevant than demyelination for determining chronic functional impairments in primary white matter diseases. Thus, serial measurement of brain N-acetylaspartate with proton MR spectroscopy can provide a reliable and clinically-relevant monitor of disease evolution. As pathological changes responsible for long-term morbidity are logically important targets for therapeutic agents, early treatment directed at axonal protection should be useful in these disorders.**  
*Journal of NeuroVirology* (2000) 6, S121–S129.

**Keywords:** N-acetylaspartate; white matter; multiple sclerosis; leukodystrophy; magnetic resonance spectroscopy

## Introduction

Magnetic resonance (MR) imaging (MRI) has provided important new insights into the understanding of multiple sclerosis (MS) (Arnold *et al*, 1997) and has proven useful in an increasing number of conditions with brain white matter (WM) pathology (van der Knaap *et al*, 1991; De Stefano *et al*, 1997). However, although conventional MRI detects brain lesions with great sensitivity, it does not provide specific information about the pathology underlying the detected WM lesions and is not a good predictor of functional impairment or disability (Arnold *et al*, 1997).

Recent years have seen the development of new MR techniques that complement conven-

tional MRI and are able to overcome some of its limitations. Proton MR spectroscopy (MRS) is one of these promising techniques and has been used recently in a number of clinical studies to supplement conventional structural neuroimaging with spatially-localised biochemical information (Arnold and Matthews, 1996). Proton MRS can provide non-invasive quantitative measurements of brain metabolites, including N-acetylaspartate (NAA), a metabolite localised almost exclusively in neurons and neuronal processes in the mature brain (Moffett *et al*, 1991; Simmons *et al*, 1991). The resonance intensity of NAA therefore provides a reliable index of neuronal integrity (Birken and Oldendorf, 1989; De Stefano *et al*, 1995b).

A number of research groups have used proton MRS and MR spectroscopic imaging (MRSI) to study patients with MS and other types of WM diseases (Arnold *et al*, 1990; Wolinsky *et al*, 1990;

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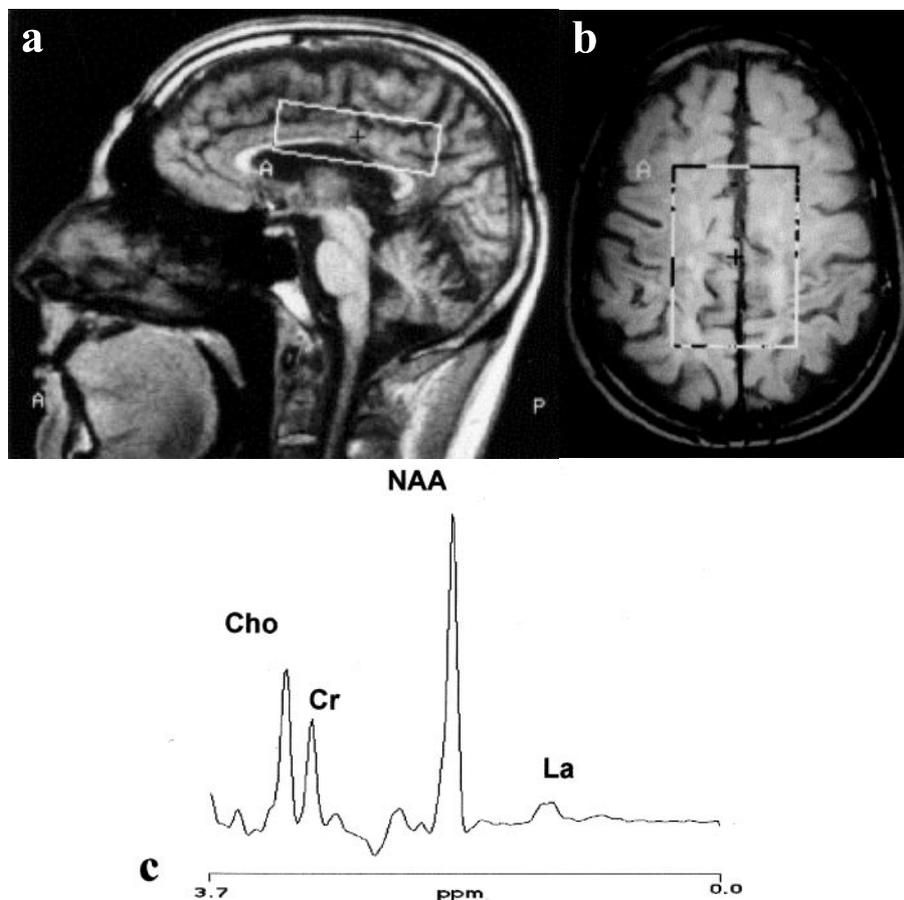
Hanefeld *et al*, 1991; Miller *et al*, 1991; van der Knaap *et al*, 1992; Kruse *et al*, 1993; Davie *et al*, 1994; Schiffmann *et al*, 1997). These MR studies have provided important insights into these disorders by emphasising axonal pathology. Here we review MRS studies assessing axonal pathology *in vivo* and present evidence indicating that axonal injury and loss may be the main link between pathological changes and the development of chronic disability.

### Introduction to proton MRS

MRS utilises the same hardware and computers as conventional MRI. However, while conventional MRI provides structural information based on signal from water, proton MRS provides measures of chemical compounds present at concentrations in the vicinity of  $10^{-5}$  that of water. MR spectra can be obtained with either single voxel (Figure 1) or spectroscopic imaging (Figure 2) methods. In both approaches, conventional MRI is performed first and used to plan the spectroscopy acquisition.

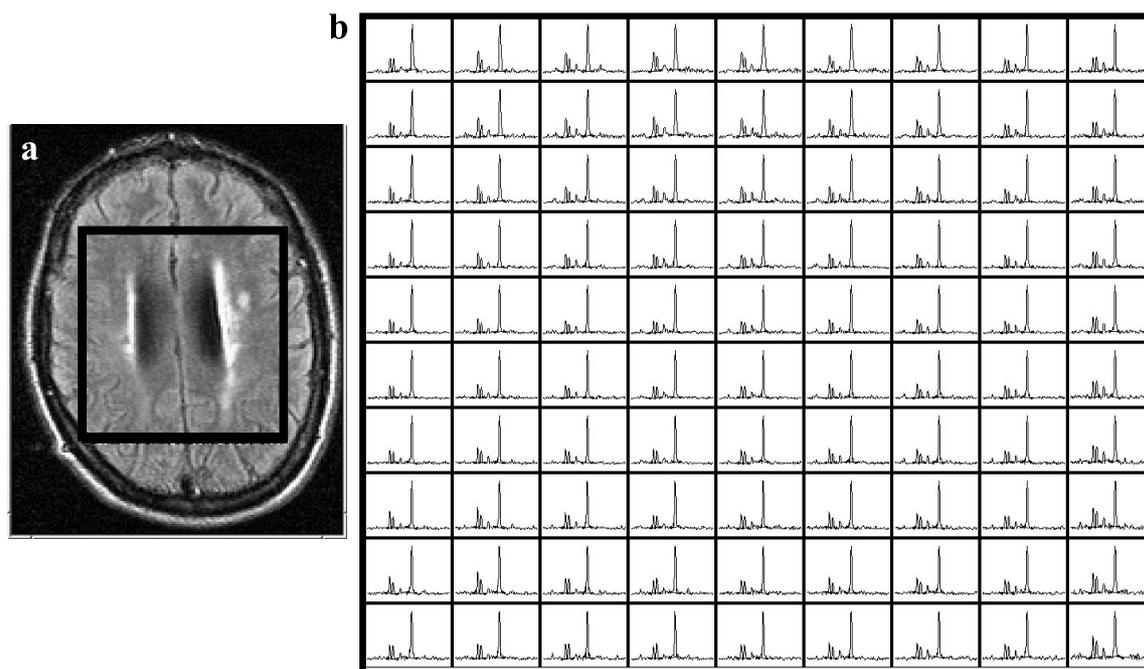
In a single voxel study one MR spectrum is obtained from a volume of interest chosen to include specifically the pathology under study. In the spectroscopic imaging approach, phase-encoding gradients are used to measure the distribution of metabolites throughout a larger volume of interest. Low-resolution images then can be generated for each metabolite by integration of the MR signals from each voxel. As spatial resolution is limited by signal intensity, the low-concentrations of brain metabolites makes the spatial resolution of the spectroscopic methods much lower than that achieved with conventional imaging based on water (70 M concentration). However, statistical inferences from the combination of the two types of MR acquisition can provide sufficiently well resolved descriptions of pathology to be useful for a broad range of applications.

Water-suppressed localised proton MRS and MRSI of normal human brain acquired at relatively long echo times (TE 136 or 272 ms) show four main peaks: (i) a large signal from N-acetyl groups (mainly NAA (Ross *et al*, 1992; Arnold and Matthews, 1996)), (ii) a smaller but still easily



**Figure 1** MRI scan in sagittal orientation (a) illustrating the volume of interest used for spectroscopy, (b) axial view of the same volume of interest and (c) proton MR spectrum from that volume of interest.

## Proton MR Spectroscopic Imaging



**Figure 2** Conventional MR imaging of a patient with multiple sclerosis in transversal orientation illustrating the volume of interest used for spectroscopy (a) and the proton spectra obtained inside this volume (b).

quantifiable resonance from choline-containing phospholipids (Cho, mainly resulting from membrane phosphocholine and glycerol-phosphocholine), (iii) creatine and phosphocreatine (Cr), which are relatively homogeneously distributed in normal brain and relatively resistant to changes (Ross *et al*, 1992; Arnold and Matthews, 1996), and (iv) lactate (Lac), which increases in concentration when oxidative metabolism cannot meet energy requirements or, acutely, in conditions associated with inflammation (Prichard, 1991; Ross *et al*, 1992). Excellent spectra can also be obtained with short echo time measurements. A greater number of metabolites (lipids, *myo*-inositol, GABA, glutamate etc.) can be detected with this method, but short echo time spectra are also much more demanding in terms of hardware, more susceptible to artifact and more difficult to quantify (Ross *et al*, 1992; Arnold and Matthews, 1996).

With both short and long echo times, the proton brain MR spectrum is dominated by the signal of NAA. Brain NAA is synthesised in neuronal mitochondria from L-aspartate and acetyl-CoA and hydrolyzed by an N-acetyl-L-aspartate amidohydrolase that is widely distributed in glial cells of the brain and in other human tissues (Birken and Oldendorf, 1989; De Stefano *et al*, 1995b). Although a number of possible functions have been suggested for NAA, its physiological role is still not known

(Birken and Oldendorf, 1989; De Stefano *et al*, 1995b). However, the fact that NAA is present almost exclusively in neurons in mature brain (Moffett *et al*, 1991; Simmons *et al*, 1991) makes it a powerful surrogate marker of neuronal damage or loss.

### NAA as marker of axonal damage in multiple sclerosis

Decreases in NAA have been observed in proton MRS studies in many pathologies associated with neuronal damage or loss (Arnold and Matthews, 1996). However, studies of NAA in patients with MS have been particularly illuminating because the extent of axonal injury associated with WM inflammation and demyelination had not been well-appreciated from classical pathology studies (McDonald, 1994; Arnold *et al*, 1997). Large decreases in brain NAA were reported in the earliest single voxel MRS studies of patients with MS (Arnold *et al*, 1990; Miller *et al*, 1991; Wolinsky *et al*, 1990; Bruhn *et al*, 1992) and confirmed in a number of more recent reports (Davie *et al*, 1994,1997; De Stefano *et al*, 1995a; Narayanan *et al*, 1997; Fu *et al*, 1998; Narayana *et al*, 1998; Sarchielli *et al*, 1999). Initial work (Arnold *et al*, 1990) also showed that greater decreases in brain

NAA were found in patients with clinically more severe disease. Since axons in the central nervous system have an extremely limited capacity for regrowth, the decreases in NAA initially were interpreted as a measure of irreversible neuronal loss. However, recovery of NAA has been reported in several conditions (Arnold *et al*, 1992; De Stefano *et al*, 1993; Lee *et al*, 1994; Vion-Dury *et al*, 1995; Matthews *et al*, 1995). Longitudinal studies of patients with demyelinating disease have emphasised that a substantial proportion of the decreases in NAA are transient in the acute phase of demyelination (Arnold *et al*, 1992; De Stefano *et al*, 1995a). Although matrix volume changes from edema may contribute to reversible decreases of NAA, the magnitude of bulk volume change is insufficient to account for the effects observed (De Stefano *et al*, 1995b). Experimental models have demonstrated clearly reversible decreases of NAA in different conditions that are not associated with volume loss. In an *in vitro* study of a neuronal cell line, a decrease in NAA was caused by serum deprivation with recovery after subsequent replacement of serum (Matthews *et al*, 1995). Reversible decreases in intracellular NAA also were shown in an *in vivo* ischaemic rat brain model (Sager *et al*, 1999). This suggests that either reversible metabolic dysfunction or considerable axonal shrinkage (as is observed immunohistochemically (Trapp *et al*, 1998)) associated with hypophosphorylation of neural filaments contribute to the observed brain NAA changes.

Early single voxel MRS studies were focused mainly on MRI-defined lesions (Arnold *et al*, 1990; Wolinsky *et al*, 1990; Miller *et al*, 1991). More recently, studies exploiting the greater coverage and resolution of MRSI have shown that the observed decreases in NAA in MS patients are not restricted to lesions, but are present both adjacent to and distant from the lesions. Group metabolite maps averaged in a standardised coordinate space have shown loss of NAA extending beyond regions of high lesion probability into surrounding regions of low lesion probability (Narayanan *et al*, 1997). Other studies have demonstrated both transient and chronic decreases in NAA in WM appearing normal on MRI (Husted *et al*, 1994; Narayanan *et al*, 1997; Davie *et al*, 1997; Fu *et al*, 1998; Narayana *et al*, 1998; Sarchielli *et al*, 1999). As axons generally project through lesions, any axonal interruption that occurs will be associated with anterograde and retrograde axonal degeneration. Therefore, it should not be surprising that axonal dysfunction or volume loss can be observed beyond the borders of MS lesions as defined by T<sub>2</sub>-weighted MRI.

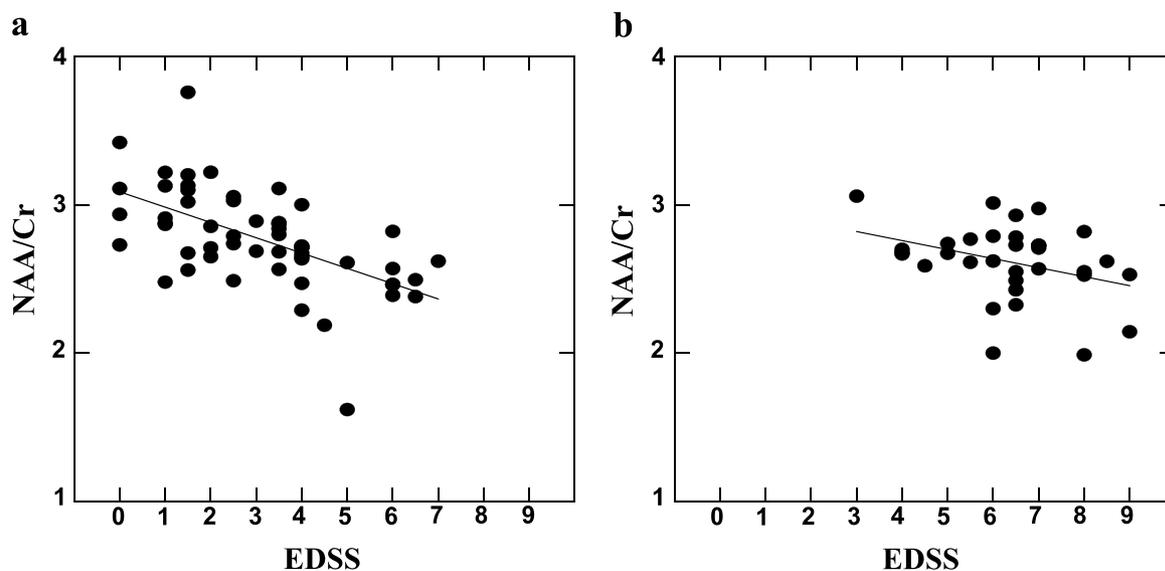
Evidence of axonal damage both in lesions and in the normal-appearing WM of MS patients also has been found in recent post-mortem studies (Davies *et al*, 1995; Trapp *et al*, 1998). Although significant axonal damage was reported in several early

pathology studies, axonal loss had been difficult to quantify with histopathology and, because of the relative prominence of demyelination, was rather neglected (McDonald, 1994). More recent pathology studies have emphasised that axonal damage does occur in MS. Axons in lesions can change in size, shape and morphology as a result of inflammation and demyelination (Prineas *et al*, 1993). Loss of axons varies considerably between lesions, being less prominent in acute lesions than in chronic lesions, and can lead to a loss of over 50% of axons (Raine and Cross, 1989; Barnes *et al*, 1991; Rodriguez and Scheithauer, 1994; Ferguson *et al*, 1997). Moreover, alterations in neurofilament phosphorylation and substantial loss of axon density can be found well outside demyelinating lesions (Trapp *et al*, 1998).

#### *Changes in NAA versus clinical disability*

The nervous system dysfunction seen in patients with MS has generally been attributed to the electrical conduction block that can occur (at least acutely) after demyelination (McDonald, 1994). However, demyelination alone is not sufficient to explain chronic disability in MS (Matthews *et al*, 1998). A dramatic illustration of this comes in a recent study which elegantly demonstrated that mice deficient in class I major histocompatibility complex (MHC) infected with Theiler's murine encephalomyelitis virus develop demyelination without neurological impairment, while class II MHC-deficient mice develop demyelination and severe neurological deficits leading to premature death (Rivera-Quinones *et al*, 1998). Studies of patients with MS suggest that diffusible factors such as reactive oxygen species or membrane-channel directed antibodies may mediate acute conduction block with WM inflammation (Youl *et al*, 1991; Utzschneider *et al*, 1993). Remyelination surely plays an important role in recovery and in longer-term trophic maintenance of axons. However, other mechanisms such as reorganisation of axon membrane sodium channels to cover demyelinated internodal regions or downregulation of inhibitory channels may be also important (Waxman, 1998). Thus, axonal adaptations alone may lead to recovery of function in regions of chronic demyelination.

As the pathological changes primarily responsible for disability are logical targets of action for new therapeutic agents, understanding the changes responsible for functional impairments is a crucial issue. Proton MRS, by providing quantitative tools for non-invasive detection of axonal injury and loss in patients with MS, allows dynamic correlations between such changes and disability in life. Recent spectroscopic studies have demonstrated highly significant correlations between decreasing NAA and increasing clinical disability in patients with isolated acute demyelinating lesions (De Stefano *et*



**Figure 3** Data illustrating the significant relationship between clinical disability (EDSS) and NAA/Cr ratios for patients with the relapsing form of multiple sclerosis ( $P < 0.001$ ) (a). This relationship is weak in patients with the secondary progressive form of multiple sclerosis ( $P > 0.1$ ) (b).

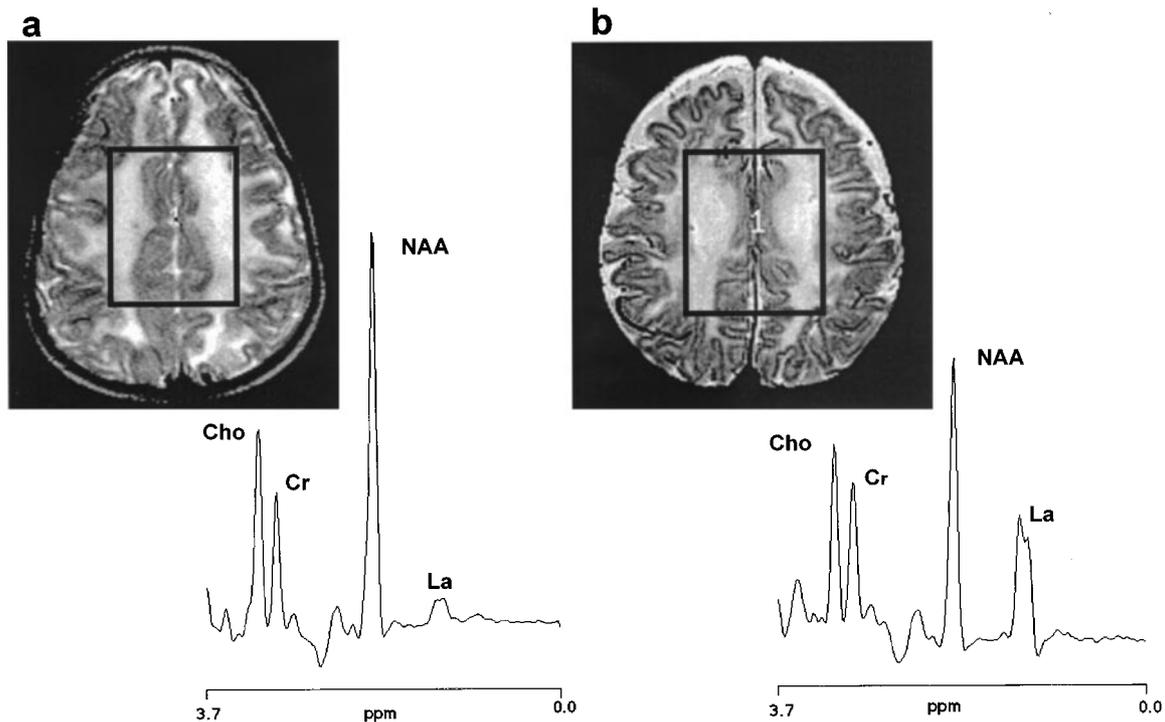
*al.*, 1995a) and in patients with established MS followed through periods of relapse and remission (De Stefano *et al.*, 1998b; Fu *et al.*, 1998) (Figure 3a). Consistent with other evidence of widespread pathology in MS, a strong correlation also was found between decreases in NAA resonance intensity and increases in clinical disability in WM appearing normal on conventional MRI (Fu *et al.*, 1998). Given that the normal-appearing WM represents by far the greatest bulk of WM, axonal loss in this brain region could be more relevant to functional impairment than axonal loss in lesions. In contrast, the correlation between NAA and clinical disability appears weak in patients with the secondary progressive form of the disease (Figure 3b), which is perhaps due to (i) the difficulty in demonstrating a relationship in this group because of a smaller slope between pathological change and disability; (ii) the greater contribution to disability of cerebral axonal pathology in the early, mild stages of MS with respect to the later, more severe stages of the disease; or (iii) the more prominent contribution of other pathological factors (i.e., spinal pathology) in the secondary progressive stage of the disease. Nonetheless, we believe that the so-called axonal hypothesis, ‘axonal damage or loss in regions of myelin or glial cell destruction is required for chronic impairments and disability’ (Matthews *et al.*, 1998), remains a powerful way of synthesising our understanding of chronic disability in MS.

The link between axonal damage and neurological impairment has been explored indirectly by other studies using MR measurements of brain and

spinal cord atrophy (Losseff *et al.*, 1996; Filippi *et al.*, 1997; Stevenson *et al.*, 1998) or hypointense lesion volumes on T1-weighted MRI (Miller *et al.*, 1998; van Walderveen *et al.*, 1998). The relationship between brain WM atrophy and axonal rarefaction or dystrophy in WM has not been defined. Preliminary data showing that brain atrophy progresses most rapidly later in the disease, while the fastest NAA loss occurs in the early stages, suggests that the two measures may be providing complementary information. A combined NAA and atrophy measure may offer a highly sensitive, clinically-relevant surrogate of pathological change useful for studying patients progressing over a broad disability range.

### NAA as marker of axonal damage in WM disorders other than MS

Brain WM disorders are a very heterogeneous group of diseases that can be due to a variety of pathological processes (autoimmune, metabolic, vascular, toxic, hereditary, etc.) and can be associated with many different types of myelin abnormality (de-myelination, hypo-myelination, myelin rarefaction, etc.) (Kolodny, 1993). The more frequent use of MRI in clinical evaluation has increased awareness for disorders involving brain WM (van der Knaap *et al.*, 1991). However, the lack of pathological specificity of conventional MRI contributes to the inability to classify many patients with these diseases. Proton MRS and MRSI, by detecting chemical-pathological changes occurring in lesions and in WM appearing normal on MRI,



**Figure 4** Conventional MRI in transversal orientation of a patient with congenital muscular dystrophy (a) and a patient with pyruvate dehydrogenase deficiency (b). MR images of both patients show similar, diffuse white matter hyperintensity. However, the MR spectrum is normal in the patient affected by congenital muscular dystrophy who did not have CNS impairment (bottom left quadrant), whereas there is a remarkable decrease in NAA and increase in Lac in the patient with pyruvate dehydrogenase deficiency who was severely neurologically impaired (bottom right quadrant).

can provide important additional information useful for diagnostic classification (van der Knaap *et al*, 1992; De Stefano *et al*, 1997).

There are several similarities between MRS findings in MS patients and in patients with other WM disorders. First, patients with acquired and hereditary WM disorders commonly show decreases in brain NAA (Kruse *et al*, 1993,1994; Tzika *et al*, 1993; van der Knaap *et al*, 1992; De Stefano *et al*, 1997). Second, in patients with WM disorders, decreases in brain NAA can be detected both in areas of hyperintense signal and in WM appearing normal on T2-weighted MRI (Kruse *et al*, 1994; De Stefano *et al*, 1997). The ubiquity of this finding suggests that some degree of axonal dysfunction and damage occurs. This is probably secondary to myelin disruption, causing a loss of trophic support for axons, and thus leading to a chronic neurodegenerative process. Third, brain NAA correlates well with the clinical status of patients affected by a variety of WM disorders. In patients with infectious disorders such as AIDS, brain NAA provided a reliable index of clinical impairment (Chong *et al*, 1993) and has been used to monitor improvements in neuronal and axonal integrity after therapeutic intervention (Vion-Dury *et al*, 1995). In a recent single voxel study performed in 12 patients with 12

different disorders presenting WM abnormalities on conventional MRI (De Stefano *et al*, 1998a), we found a very close relationship between NAA values from central brain regions and patients' CNS impairment (computed using the Functional Status Score (Kurtzke, 1983)). Data from this study showed that brain NAA and patients' CNS impairment may be correlated in circumstances in which there is no relationship between the clinical status and the degree of WM changes on conventional MRI (Figure 4).

## Conclusions

There is enough MR and pathological evidence that progressive accumulation of disability in patients with MS and other WM disorders reflects chronic, progressive damage to axons. This has obvious implications for the development of new therapeutic approaches.

Proton MRS can provide *in vivo* measurement of brain NAA, an index of axonal integrity, allowing accurate monitoring of disease evolution and response to therapeutic intervention. Combining MRS with measures derived from conventional structural imaging (e.g., lesion volume, brain and

spinal cord atrophy measurements) can provide a more complete description of the dynamics responsible for pathological changes as well as a more accurate evaluation of disease progression and response to therapy.

## Acknowledgements

The study was supported in part by grants from the Multiple Sclerosis Society of Canada and from

the Progetto Sclerosi Multipla of the Istituto Superiore di Sanita', Rome. PM Matthews and DL Arnold gratefully acknowledge support from the Medical research Councils of the UK and Canada, respectively.

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